

Partial-Fourier Reconstruction for Functional MRI(fMRI) using Deep Learning

Department of Electrical Engineering

Seul Lee (seul@stanford.edu)

Functional Magnetic Resonance Imaging (fMRI) is an MRI method for looking at brain functional connectivity by detecting blood flow changes. To reduce scan time, Partial Fourier reconstruction that acquires partial number of k-space data is widely used and reconstruct images using Hermitian symmetry. We proposed new Partial Fourier reconstruction method in other research: Even/Odd (E/O) reconstruction. In this method, as there are every other lines in k-space, the missing voxels can be filled using nearby voxels. In this project, I used deep learning algorithm to compensate missing k-space voxels by training nearby voxels.

Data acquisition

- · The fMRI data were acquired at 3T GE scanner at Lucas center with TR/TE = 2100/20 ms, 3.4 mm resolution and 4 mm slice thickness. k-Space data consists of $64 \times 64 \times$ number of planes in slice (z) direction (64×64 matrices
- Number of rows = 64, number of columns = 41/64, number of slice = 30

Preprocessing

- · FFT was applied to transform between k-space and images
- · Magnitude/phase were separated and normalized
- · Zero-out every other lines from each half keeping the center lines

Features/Labels

- Features: k-space values at acquired voxels
- · Labels: the values at missing voxels
- Row: two position values in k-space,
- Column: number of datasets (each point in k-space)

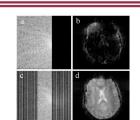


Figure 1. Concepts of partial Fourier acquisition:

Homodyne [1] (a,b), E/O (c,d)

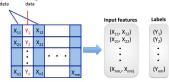


Figure 2. Data structure

Models

Models

- · Motivation: Filling missing lines using neighboring voxels works well
- · Linear-tanh-inear-tanh model is applied

Activation functions: relu for magnitude and tanh for phase

 $(\exp(z) - \exp(-z))$ • Linear: $Z_i = W_i X_i + b_i$, Relu: $G(Z_i) = \max(0, Z_i)$, $\tanh(z) =$ $(\exp(z) + \exp(-z))$

W1: [16, 2], W2: [8, 16], W3: [1, 8]

tanh activation

Relu activation



Figure 3. Model structure. n = 2, m = 236160 in X_{nm} and Y_{nm}

Optimization

Gradient descent optimizer

Results

Post-processing

- · Obtained data were filled in the original position in k-space
- · IFFT was applied to reconstruct brain images

(a) Fully sampled





Evaluation

Mean Squared Error (MSE) between labels and predictions

		Training	Test
	Dataset	138,240 positions	1,536 positions
0)	MSE	0.038 (mag) 0.317 (phs)	0.048 (mag) 0.319 (phs)

Acknowledgement

Thanks to my project TA Brandon Chauloon Yang and Gary Glover for helpful discussion and comments.

[1] Noll DC, Nishimura DG, Macovski A. Homodyne detection in magnetic resonance imaging. IEEE Trans Med Imaging 1991;10(2):154-63.

Discussion

Figure 4. Reconstructed images from

fully acquired data (a) and tested data(b

- Since neighboring voxels are correlated in MR images, they can be used to compensate missing k-space data in E/O reconstruction. In this project, the missing voxels were filled using deep learning algorithm.
- In the future, instead of point to point learning, CNN can be used for training whole k-space to reconstructed images, which is an end-to-end application.